



PCT/GB2004/02363



INVESTOR IN PEOPLE

The Patent Office
Concept House
Cardiff Road
Newport
South Wales
NP10 8QQ

REC'D 13 JUL 2004

WIPO

PCT

I, the undersigned, being an officer duly authorised in accordance with Section 74(1) and (4) of the Deregulation & Contracting Out Act 1994, to sign and issue certificates on behalf of the Comptroller-General, hereby certify that annexed hereto is a true copy of the documents as originally filed in connection with the patent application identified therein.

In accordance with the Patents (Companies Re-registration) Rules 1982, if a company named in this certificate and any accompanying documents has re-registered under the Companies Act 1980 with the same name as that with which it was registered immediately before re-registration save for the substitution as, or inclusion as, the last part of the name of the words "public limited company" or their equivalents in Welsh, references to the name of the company in this certificate and any accompanying documents shall be treated as references to the name with which it is so re-registered.

In accordance with the rules, the words "public limited company" may be replaced by p.l.c., plc, P.L.C. or PLC.

Registration under the Companies Act does not constitute a new legal entity but merely subjects the company to certain additional company law rules.

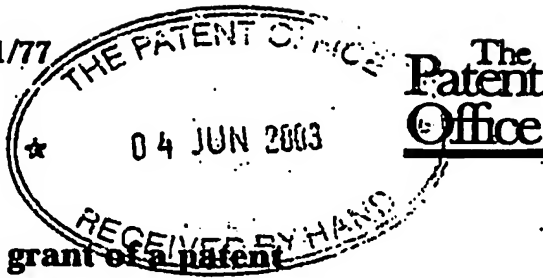
Signed

He Behen

Dated

6 July 2004

PRIORITY DOCUMENT
SUBMITTED OR TRANSMITTED IN
COMPLIANCE WITH
RULE 17.1(a) OR (b)



1777
POL 7760 000-0512918.8

Request for grant of a patent

(See the notes on the back of this form. You can also get an explanatory leaflet from the Patent Office to help you fill in this form)

The Patent Office

Cardiff Road
Newport
South Wales
NP9 1RH

| | | | |
|-----------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------------|-----------------------------------------------------------------------------------------------------|-------------------------------------------------|----------------------------------------|
| 1. Your reference | SAH02670GB | | |
| 2. Patent application number (The Patent Office will fill in this part) | 0312818.8 | | e. 4 JUN 2003 |
| 3. Full name, address and postcode of the or of each applicant (underline all surnames) | Cambridge University Technical Services Ltd The Old Schools Trinity Lane Cambridge CB2 1TS | | |
| Patents ADP number (if you know it) | 6956809004 | | |
| If the applicant is a corporate body, give the country/state of its incorporation | United Kingdom | | |
| 4. Title of the invention | Acoustic Sensor | | |
| 5. Name of your agent (if you have one) | Gill Jennings & Every | | |
| "Address for service" in the United Kingdom to which all correspondence should be sent (including the postcode) | Broadgate House 7 Eldon Street London EC2M 7LH | | |
| Patents ADP number (if you know it) | 745002 | | |
| 6. If you are declaring priority from one or more earlier patent applications, give the country and the date of filing of the or of each of these earlier applications and (if you know it) the or each application number | Country | Priority application number (if you know it) | Date of filing (day / month / year) |
| 7. If this application is divided or otherwise derived from an earlier UK application, give the number and the filing date of the earlier application | Number of earlier application | | Date of filing (day / month / year) |
| 8. Is a statement of inventorship and of right to grant of a patent required in support of this request? (Answer 'Yes' if: a) any applicant named in part 3 is not an inventor, or b) there is an inventor who is not named as an applicant, or c) any named applicant is a corporate body. See note (d)) | YES | | |

Patents Form 1/77

9. Enter the number of sheets for any of the following items you are filing with this form. Do not count copies of the same document

Continuation sheets of this form

| | |
|-------------|----|
| Description | 12 |
| Claim(s) | 4 |
| Abstract | |
| Drawing(s) | 4 |

10. If you are also filing any of the following, state how many against each item.

Priority documents

Translations of priority documents

Statement of inventorship and right to grant of a patent (*Patents Form 7/77*)

Request for preliminary examination and search (*Patents Form 9/77*)

Request for substantive examination (*Patents Form 10/77*)

Any other documents
(*please specify*)

NO

11. For the applicant
Gill Jennings & Every

I/We request the grant of a patent on the basis of this application.

Signature

Date

Michael J. ... June 2003

12. Name and daytime telephone number of person to contact in the United Kingdom

HALEY, Stephen
020 7377 1377

Warning

After an application for a patent has been filed, the Comptroller of the Patent Office will consider whether publication or communication of the invention should be prohibited or restricted under Section 22 of the Patents Act 1977. You will be informed if it is necessary to prohibit or restrict your invention in this way. Furthermore, if you live in the United Kingdom, Section 23 of the Patents Act 1977 stops you from applying for a patent abroad without first getting written permission from the Patent Office unless an application has been filed at least 6 weeks beforehand in the United Kingdom for a patent for the same invention and either no direction prohibiting publication or communication has been given, or any such direction has been revoked.

Notes

- If you need help to fill in this form or you have any questions, please contact the Patent Office on 0645 500505.
- Write your answers in capital letters using black ink or you may type them.
- If there is not enough space for all the relevant details on any part of this form, please continue on a separate sheet of paper and write "see continuation sheet" in the relevant part(s). Any continuation sheet should be attached to this form.
- If you have answered 'Yes' Patents Form 7/77 will need to be filed.
- Once you have filled in the form you must remember to sign and date it.
- For details of the fee and ways to pay please contact the Patent Office.

ACOUSTIC SENSOR

Acoustic sensors which employ resonators have been used as detection devices for biological molecules for the past two decades, exhibiting sensitivity in the ng/ml range. They share with optical devices an ability to produce evanescent waves that propagate a limited distance across the solid liquid interface, so molecular events and processes in the bulk are not detected; only those processes leading to interfacial elasticity, viscosity, viscoelasticity and slippage are detected.

However there are significant problems with these systems. As the dimensions of the molecules of interest range from 5 to 20 nm, a substantial amount (> 95%) of acoustic transverse coupling is to the fluid above the chemical interface, essentially outside of the domain of the analysis in which there is interest.

An evanescent sensing region that is significantly thicker than the chemical layer of interest leads to reduced sensitivity and interpretation complications. For example, optical SPR (surface plasmon resonance) sensors generate a 200 nanometre evanescent wave, that is supposed to measure the refractive index of the protein layer, and yet it is the composite refractive index of the film and more significantly the fluid that is determined. Similarly electroded piezoelectric crystals known as TSMs (thickness shear mode) or QCMs (quartz crystal microbalances) operate at 10 MHz, which also have an evanescent penetration depth that reaches beyond the chemical layer of interest. Focusing the evanescent wave towards the interface has been attempted with magnetic acoustic resonance sensors that work at 50 MHz, however wave penetration still overshoots the interfacial chemistry with losses in sensitivity. Surface acoustic wave devices known as the Love wave device can work at higher frequencies for smaller penetration depths, however none of these systems provide a sufficiently compact evanescent zone to fully recover the biochemical signal.

A further restriction of these sensors is that a very limited window of information is recovered, at a single wavelength or frequency. This is tantamount to operating an IR spectrometer at a single wavelength, which severely
5 reduces the value of the data recovered.

With respect to the practical format of these systems, all optical and acoustic devices require additional layers of metallisation to be applied and patterned, which for the interdigitated pattern on SAW (surface acoustic wave) is an
10 especially costly process. In use optical sensing systems require careful alignment and isolation from sources of vibration. Whilst the materials used in MARS (magnetic acoustic resonance sensor) and SAW are sensitive to temperature and demand careful environmental control in
15 order to function without signal drifts. Wire connections to QSM and SAW devices are required, which reduces compatibility with chemical immobilisation modifications and procedures and places design constraints on commercial instruments.

20 The present invention aims to overcome the above limitations of conventional acoustic sensors.

According to the present invention there is provided an acoustic sensor comprising:

at least one resonant element;

25 a driver comprising an electrical coupling means and an electromagnetic field source, arranged such that, in use, the electrical coupling means transfers current to the electromagnetic field source to produce an electromagnetic field that drives the at least one resonant element to
30 produce acoustic waves directed to a predetermined part of a test sample;

an electromagnetic detector arranged to receive, in use, the acoustic spectrum emitted from the test sample after the acoustic waves have interacted with the test
35 sample; and

an electrical circuit connected to the driver and electromagnetic detector, the circuit arranged, in use, to provide the current and to detect, in combination with the

electromagnetic detector, the acoustic spectrum received by the electromagnetic detector.

According to the present invention there is also provided a method for use in acoustic sensing, the method comprising the steps of:

applying a current to an electrical coupling means; transferring current from the electrical coupling means to an electromagnetic field source;

driving, with an electromagnetic field produced by the electromagnetic field source, at least one resonant element to produce acoustic waves to interrogate a test sample; and

detecting with an electrical circuit connected to an electromagnetic detector and the electrical coupling means, the acoustic spectrum produced after the acoustic waves have interacted with the test sample.

An example of the present invention will now be described with reference to the accompanying drawings, in which:

Figure 1a shows an example spiral coil structure according to the present invention and Figure 1b shows an example coil and piezoelectric crystal according to the present invention, with electromagnetic field lines shown;

Figure 2 shows an example based on a MARS signal generator and lock-in amplifier detector system used to generate and detect the acoustic signals according to the present invention and the electrical equivalent circuit of the coaxial cable and spiral coil;

Figure 4 indicates the wide bandwidth of the system by comparing acoustic resonance envelopes detected in the a) ultrasonic to b) hypersonic range for a quartz disc in contact with deionised water;

Figure 5 shows the complete acoustic signal spectrum of two different examples of 0.25mm quartz discs in contact with deionised water, as measured with our described electrical system without any mechanical or electrical tuning of components;

Figure 6 shows the variation in a) acoustic Q factor and b) the evanescent wave depth with operating frequency for a quartz disc in contact with deionised water; and

Figure 1b and Figure 2 show an example arrangement in a sensor according to the present invention. A coil 1 receives RF current 4 via a multiply resonant transmission line 6. The electromagnetic field 5 produced by the coil 1 drives a piezoelectric element 3 to produce acoustic waves by electrostriction. The sensing done by the acoustic waves occurs either directly or indirectly. The substance to be detected either adsorbs to the vibrating surface, or a receptor can be attached to the vibrating surface, which is specific to the substance to be detected. When the substance adsorbs, it changes the acoustic spectrum. The coil 1 also acts as a detector, which converts the changed electromagnetic field caused by the changed acoustic waves back into a RF current which is detected by a detection circuit, which includes an AM-diode detector 7 in this example.

The present invention eliminates the need for fine tuning between the transmission line 6 and the coil 1 in order to generate the desired acoustic waves, and acoustic waves which penetrate to the layer of interest can be produced. Also, acoustic waves with a wide range of frequencies can be produced.

The sensor can be used to detect substances such as cells, proteins, antibodies and nucleic acids.

We have identified that the problem of low frequency of operation of current acoustic resonant devices is not to do with the material, but with how the material is excited.

The opportunity to focus evanescent waves substantially to the chemical interface, and enhance molecular coupling, is exemplified by the low intrinsic loss of amorphous glasses and single crystal materials, which supports operation at GHz frequencies.

In terms of coupling processes that have been used to date to excite magnetic films and piezoelectric crystals, the presence of the sample in the electromagnetic field to

excite acoustic waves /phonons has been sufficient to achieve generation in the hypersonic GHz range. In contrast, known acoustic sensor configurations rely on electrical signals transmitted through wires to metal electrodes in order to excite the acoustics. This has continued with surface acoustic waves devices, which obtain higher frequencies of operation, but these are still inconvenient for locating hypersonic transverse waves that can concentrate at the molecular interface. This coupling limitation of the electrode to low frequencies, has been addressed in the present invention by providing an alternating electric or magnetic dipole constructed, for example, from a spiral coil 1, that has many attractive measurement properties. Alternatively, the coil 1 could be replaced by a linear electric dipole and the same function achieved at a different signal to noise ratio. A primary advantage is ultrasonic generation in a wide variety of substrates and composites that include metals, glasses, sapphire, diamond, silicon, quartz, lithium niobate, lithium tantalate, and nickel, simply by placing the substrate material above the coil. For substrates of low intrinsic loss such as amorphous and single crystal resonators, piezoelectricity, magnetostriction and magnetic direct generation can be used to initiate coupling at different frequencies, in order to provide new molecular information from transverse wave coupling at the solid-liquid interface. The only substrate materials that cannot be acoustically excited with a coil are insulators which do not incorporate any magnetic or electric dipoles or any conductive region. Therefore the resonant element 3 can be made of one of a wide range of materials or a combination of several. It can be any material with magnetic or electric dipoles that acquires energy from the electrical or magnetic components of the radio frequency electromagnetic waves and translates that acquired energy into acoustic motion, preferably as a standing wave in the material.

The present invention is the result of optimising the electrical configuration so coupling between the dipoles instigated in an electromagnetic source such the spiral coil 1 and dipoles in a material element lead to wideband ultrasonic and hypersonic evanescent wave generation. We have determined that the electrical circuit components are very important in enabling or restricting the flow of RF current to the coil, so fluctuations in the magnitude of these currents due to the acoustic generation process can be measured.

In order to generate hypersonic evanescent waves an examination of the electrical impedance of the components that will transfer current from the signal generator to the spiral coil antenna is important. The strategy used in the invention is to take the MARS system which has already been developed for spiral coil operation, and improve it so that there is no need for mechanical tuning. In the prior art, a capacitor mounted alongside the coil is used to establish electrical parallel resonance, which not only requires significant time to match the electrical and acoustic resonance frequencies, but also tends to quench the resonance due to dielectric loss in the capacitor. The present invention avoids this by the tuning capacitor being dispensed with entirely, relying on the characteristics of a transmission cable 6 between the coil and the signal source. At these high frequencies each connection that would be ignored at lower MHz frequencies now becomes an important component of the signal-to-noise ratio of the system.

The preferred embodiment of the present invention uses a MARS system with a sensitive detection circuit that uses a differential amplifier and synchronous receiver to recover acoustic signals without contacting the vibrating elements, although any means that can generate radio frequency currents and detect them in the MHz to GHz range can be used. In this embodiment, the coil carries out the electromagnetic detection function as well as the electromagnetic field source function. This does not have

to be the case. The electromagnetic field source and detector can be two different elements. The differential amplifier operates to increase the received signal, and at the same time, subtract away the unwanted transmitted signal, whilst the synchronous receiver follows on by eliminating external noise through a process of very narrow bandwidth filtering, so high signal-to-noise ratios can be recovered from the sensing device.

In an example of the present invention, AT cut 6 MHz 0-25mm piezoelectric crystals are contained in a flow through cell into which a spiral coil 1 element had been incorporated. An E8254A signal generator (40 GHz) is used to supply a frequency modulated RF signal 4 to the coil 1, whilst an in-house differential AM detector 7 and the EG&G lock-in amplifier extract the acoustic signal. See Figure 1. The coil 1 is on a supporting epoxy laminate board 2. All of the harmonic frequencies of the crystal are collected by continuously scanning the resonance amplitudes from 6 MHz to 1.1 GHz over precisely defined frequency intervals. An HP impedance analyser with a 16992A test set is used to characterise the electrical impedance of the coil and transmission line, so the acoustic response can be interpreted. Directly using an impedance analyser is an alternative to a modified MARS system.

As the MARS system operates at several different harmonic frequencies, the electrical conditions and their contribution at the different frequencies to current through the coil are very important to system behaviour, particularly to the signal-to-noise ratio at hypersonic frequencies. For this reason the calculated and measured electrical impedance of the coil and the transmission line are used as a backcloth from which to interpret the acoustic data.

Although a coil is used in this embodiment, the electromagnetic field source can be other inductors or means to produce a radio frequency electromagnetic waves from a radio frequency current, such as a single wire or a microwave horn. Similarly, a transmission line is not the

only possible electrical coupling means that could be used. It could be any hard wire connection that links the electromagnetic field source to the electrical circuit and induces standing waves.

5 As shown in Figure 1, the spiral coil 1 is used to induce an RF electrical field 5 in a piezoelectric plate 3, and can be described by an equivalent circuit of impedance Z_R

$$Z_R = \left(j\omega C + \frac{1}{R_L + j\omega L} + \frac{1}{R_p} \right)^{-1}$$

10 comprising a capacitor (1.7 pF), inductor (1.15 uH) a wire resistance (5 Ohm) and parallel resistance (8000 Ohm) as indicated in Figure 2. For a 30 turn coil made from 0.085 mm enamelled copper wire a precise fit between the calculated and experimental response, determined via the HP
15 impedance analyser (4291B), can be obtained. A comparison with an electroded TSM 6.5 MHz device indicates the large difference in impedance between capacitive and inductively coupled crystals, indicating that electrical conditions for acoustic detection will necessarily be different in these
20 two cases. One key difference understood from the equivalent circuits, is that the coil exhibits a parallel electrical resonance, even when no capacitance is directly attached to the coil. This behaviour is a due to interwinding and substrate capacitance, which may shunt valuable
25 current away from driving of the acoustic resonance and contribute to dielectric losses at hypersonic frequencies. However as quick recovery of data over a wide bandwidth is desirable, time consuming manual tuning of the electrical characteristic is avoided by using a multiply resonant
30 coaxial transmission line 6, or other electrical coupling means, between the coil and detector.

Because of its repeating electrical impedance, the coaxial line 6 transfers RF current over a wide bandwidth without a deleterious matching losses. For this reason it
35 effectively replaces the capacitor used with the original

MARS system, which acts as a current shunt at high frequency. The impedance of the transmission line 6 can be calculated from Z.

$$5 \quad Z = Z_0 \left[\frac{(Z_R / Z_0) + \tanh[\gamma d]}{1 + (Z_R / Z_0) \tanh[\gamma d]} \right]$$

where $\gamma = \sqrt{(R + j\omega L)(G + j\omega C)}$ and $Z_0 = \sqrt{(R + j\omega L) / (G + j\omega C)}$,

and d is the length of the line 6 and shown to fit our experimental data when $R=0.1$ ohm, $L=0.23\mu\text{H}$, $C=55\text{pF}$ and $G=10^{-9}$. Its repeat behaviour is due to the electromagnetic standing wave condition in the line, which leads to multiple resonances similar to acoustic resonance, however the lower electrical Q factor leads to impedance fluctuations of the line staying within a specified range. This prevents severely mis-matched electrical conditions from arising, whilst retaining simplicity without the need for manual tuning. These coaxial line resonances therefore assist acoustic detection at a very high frequencies.

Current transferred to the coil 1 due to the combined response of the coil 1 and coaxial line 6 can be calculated by adding the real and imaginary parts of the coil and line impedance together, to give the overall impedance connected to the detector. To predict the acoustic behaviour with frequency, it is necessary to use the impedance formula for the coil to determine the consequence of a radiation resistance, that appears at the acoustic resonance frequency. This resistance is in series with the wire resistance and describes the loss of power to the acoustic resonance. Assuming the radiation resistance due to the acoustic generation is constant with frequency, it can be demonstrated that the acoustic response appears as measurable fluctuations in the electrical impedance.

The basis to acoustic generation is the electrical current following through the coil and the transmission line and its interaction with the magnetic or electric

dipoles in the disk. Here current driven through the electrical network to the coil 1, leads to a varying magnetic field (Ampere's law) and in turn an electrical field 5 (Faraday's law) which forces dipoles into motion.

5 In the example presented here, this process is the dipoles in the piezoelectric disc 3 being driven by an electric field via electrostriction, effectively a change in dimension of the disc within the field. For acoustic generation across many frequencies, the following
10 conditions must be satisfied: (1) sufficient current must be available in the windings of the spiral coil (2) the resulting electrical fields must be predominantly perpendicular to the plane of the disk (AT piezoelectric crystal only) (3) the acoustic loss needs to be minimal.
15 Placing energy in the acoustic spectrum is critically dependent on the coil construction, and the highest frequency of generation desired.

As indicated above, acoustic generation at hypersonic frequencies depends on satisfying key criteria, which we
20 now relate to our measured acoustic response (Figure 5) detected with the FM signal generator and AM detector, lock in amplifier receiver (Figure 2).

A simple acoustic amplitude is not measured but the differential of the amplitude with respect to frequency
25 (Figure 5). This behaviour arises as the changes in the frequency of the signal via FM modulation produces a low noise AM signal only if the electrical impedance fluctuates rapidly with frequency: a situation brought about by any high Q acoustic resonance (10^3 - 10^4). So overall, the
30 differential of the acoustic amplitude with frequency is what is being detected, for the reason that much higher signal-to-noise ratios of >3000 up to 600MHz can be achieved than by directly measuring the amplitude. For example in the alternative measurement format where direct
35 connection is made between the coil and the impedance analyser, then resolution of many of the resonance envelopes is not possible due to low signal-to-noise conditions, however improved coil construction may make

this option a useful approach. As frequency is a fundamental determinant of the response, the spectrum contains a lot of information about to the behaviour of the system and how the electrical network can lead on to hypersonic operation.

Each of the resonances in Figure 5 fits precisely to anticipated shear wave resonance frequencies, as a precise frequency interval of 13.21380 MHz is measurable across the series. The velocity calculated from this value is 3750 ms⁻¹, which is the shear wave velocity of an AT crystal, which shows the acoustic shear wave harmonics are being detected by the MARS system.

Beyond N = 61, a periodicity in the envelope of the peak amplitude becomes obvious. This is related simply to the length of the coaxial line.

As can be seen from figure 5, the vertical bars are all separated by exactly the same frequency, indicating that the shear harmonic mode is what is being collected. However this incremental behaviour does not cease, but continues throughout the trace to a lift in the resonance envelope at 1.0902 GHz. This shows that hypersonic signals are being generated.

On selecting harmonic No. 165, a smooth resonance contour was found that does not have the regular and harmonic responses associated with non plane parallel surfaces. The fact that an acoustic resonance had been detected was supported by the measured Q factor, which was consistent with the rest of the family of shear wave resonances observed. As further confirmation that acoustic harmonic signals are being monitored over multiple frequencies where evanescent wave depth decreases with frequency, a solution of IgS was injected at 1000µg/ml. Figure 6 shows that the frequency a) and amplitude b) is shifted in a frequency dependent manner. Figure 6c) shows how the frequencies relate to the evanescent penetration depth.

An effective method for ultrasonic and hypersonic generation at the solid liquid interface without mechanical

tuning has been demonstrated, with acoustic losses consistent with superior coupling to a chemical recognition layer, and less radiation into the overlying supernatant. This process uses simple system components, such as a hand wound coil, lock-in amplifier and signal generator. For sensing applications many different chemical recognition systems can be immobilised on the sensing element involving antibodies, cells, nucleic acids and the acoustic fingerprint or spectra used to extract changes in conformation and composition of a nanoscale film. The ability to select different operating frequencies with this approach, can be used to explore ultrasonic and extended hypersonic changes in surface stress, relaxation, and slippage of a nanoscale film to provide a new tool for drug discovery and clinical diagnostics.

13
CLAIMS

1. An acoustic sensor comprising:
at least one resonant element;
5 a driver comprising an electrical coupling means and
an electromagnetic field source, arranged such that, in
use, the electrical coupling means transfers current to the
electromagnetic field source which produces an
electromagnetic field that drives the at least one resonant
10 element to produce acoustic waves directed to a
predetermined part of a test sample;
an electromagnetic detector arranged to receive, in
use, the acoustic spectrum emitted from the test sample
after the acoustic waves have interacted with the test
15 sample; and
an electrical circuit connected to the driver and
electromagnetic detector, the circuit arranged, in use, to
provide the current and to detect, in combination with the
electromagnetic detector, the acoustic spectrum received by
20 the electromagnetic detector.
2. A sensor according to claim 1, wherein the electronic
circuit comprises an electrical oscillator.
- 25 3. A sensor according to claim 1, wherein the electronic
circuit comprises a frequency modulated signal generator,
an AM diode detector and a lock-in amplifier.
4. A sensor according to any preceding claim, wherein the
30 electromagnetic field source and the electromagnetic
detector are the same member.
5. A sensor according to any preceding claim, wherein the
electromagnetic field source is single wire.
- 35 6. A sensor according to any of claims 1 to 4 wherein the
electromagnetic field source is a coil.

7. A sensor according to claim 6, wherein the coil is spiral.
8. A sensor according to claim 6 or claim 7, wherein the
5 coil is copper.
9. A sensor according to claim 7 or 8, wherein the coil is formed from wire wound into a flat spiral element.
- 10 10. A sensor according to any of claims 1 to 4, wherein the electromagnetic field source is a microwave horn.
11. A sensor according to any of the preceding claim, wherein the electromagnetic detector is single wire.
- 15 12. A sensor according to any of claims 1 to 10, wherein the electromagnetic detector is a coil.
13. A sensor according to claim 12, wherein the coil is
20 spiral.
14. A sensor according to claim 12 or claim 13, wherein the coil is copper.
- 25 15. A sensor according to claim 3 to 14, wherein the coil is formed from wire wound into flat spiral element.
16. A sensor according to any of claims 1 to 10, wherein the electromagnetic detector is a microwave horn.
- 30 17. A sensor according to any of claims 1 to 16, wherein the resonant element is metal.
18. A sensor according to any of claims 1 to 17, wherein
35 the resonant element is magnetostrictive.
19. A sensor according to any of claims 1 to 16, wherein the resonant element is piezoelectric.

20. A sensor according to any preceding claim, wherein the resonant element is a composite of at least two different materials.

21. A sensor according to any preceding claim, wherein the test sample is in the gaseous phase.

22. A sensor according to claim 21, wherein the resonant element is coated with a polymer layer.

23. A sensor according to any preceding claim, wherein the test sample is in the liquid phase.

24. A sensor according to any preceding claim, wherein the electrical coupling means is a multiply resonant transmission line.

25. A sensor according to any preceding claim, wherein the resonant element is coated with a biorecognition layer.

26. A sensor according to any one of the preceding claims, wherein in use, the sensor detects cells.

27. A sensor according to any of claims 1 to 25, wherein in use, the sensor detects proteins.

28. A sensor according to any of claims 1 to 25, wherein in use, the sensor detects antibodies.

29. A sensor according to any of claims 1 to 25, wherein in use, the sensor detects nucleic acids.

30. A method for use in acoustic sensing, the method comprising the steps of:

applying a current to an electrical coupling means;
transferring current from the electrical coupling means to an electromagnetic field source;

driving, with an electromagnetic field produced by the electromagnetic field source, at least one resonant element to produce acoustic waves directed to a predetermined part of a test sample; and

- 5 detecting with an electronic circuit connected to the electromagnetic field source together with an electromagnetic detector and the electrical coupling means, the acoustic spectrum produced after the acoustic waves have interacted with the test sample.

10

31. A method according to claim 30, wherein the at least one resonant element produces acoustic waves by electrostriction.

15

32. A method according to claim 30, wherein the at least one resonant element produces acoustic waves by magnetostriction.

20

33. A method according to any of claims 30 to 32, wherein the acoustic waves are detected by means of an electrical oscillator tuned to the fundamental or harmonic frequency of the resonant element.

25

34. A method according to any of claims 30 to 32, wherein the acoustic waves are detected by means of a frequency modulated signal generator, an AM diode detector and a lock-in amplifier.

FIGURE 1 a

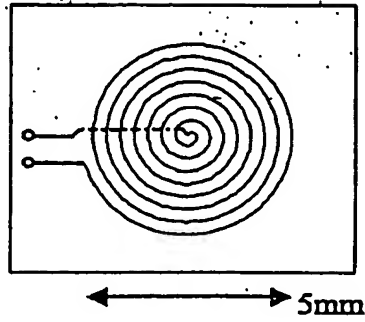


FIGURE 1 b

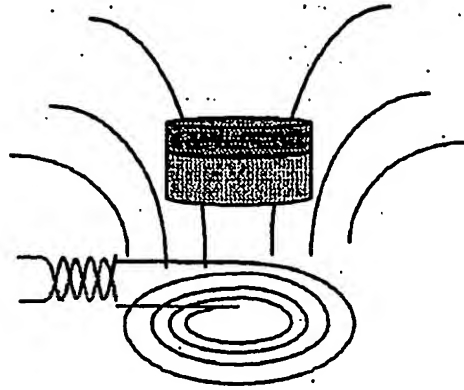
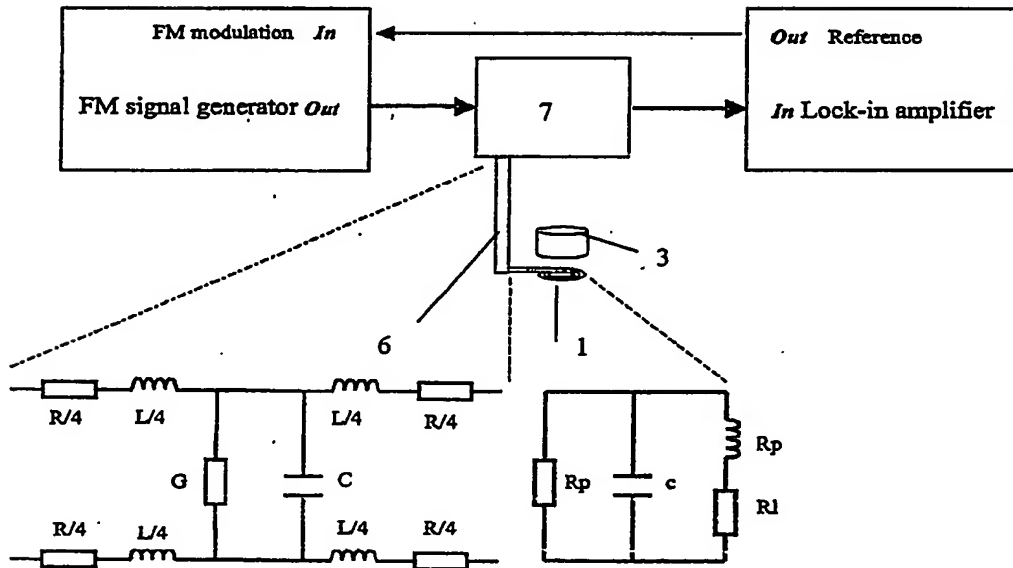


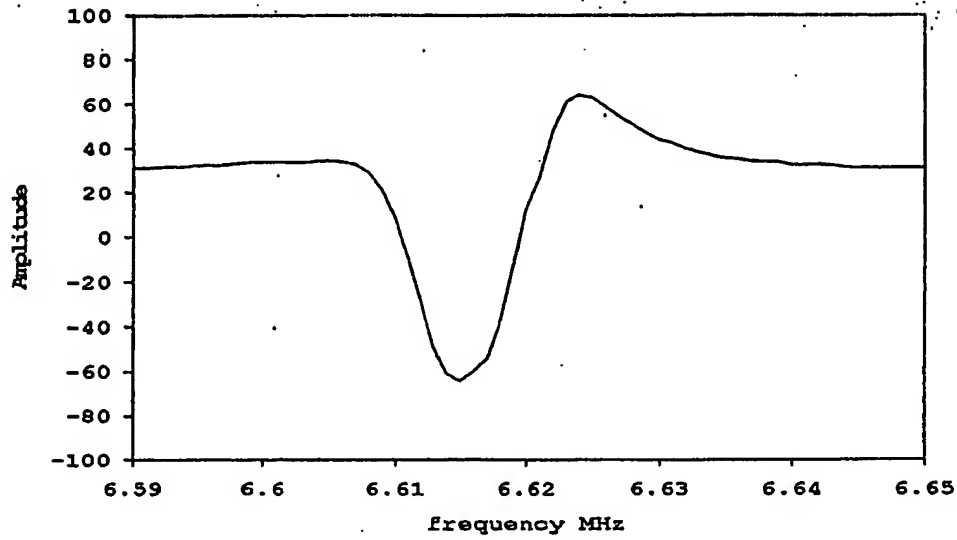
FIGURE 2



2/4

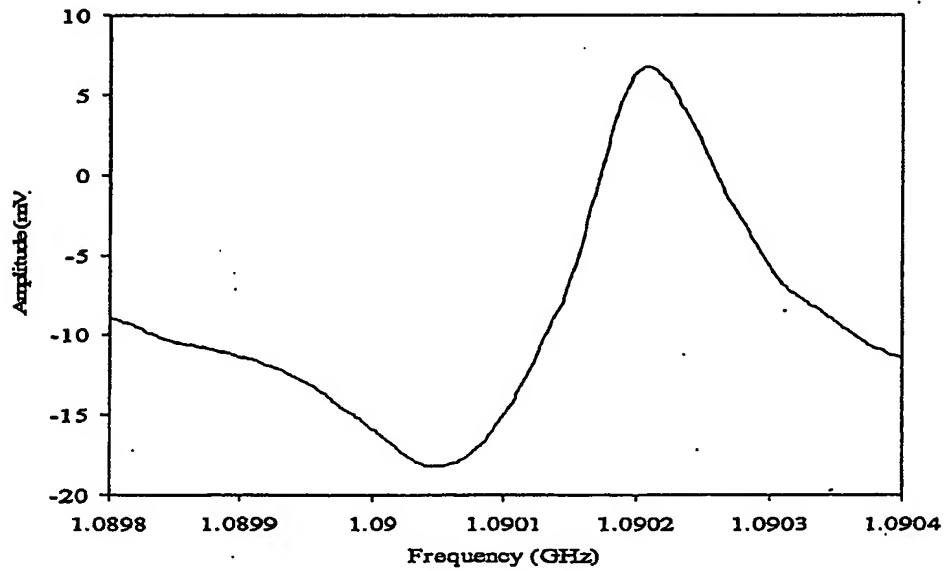
FIGURE 3

6.6 MHz



b)

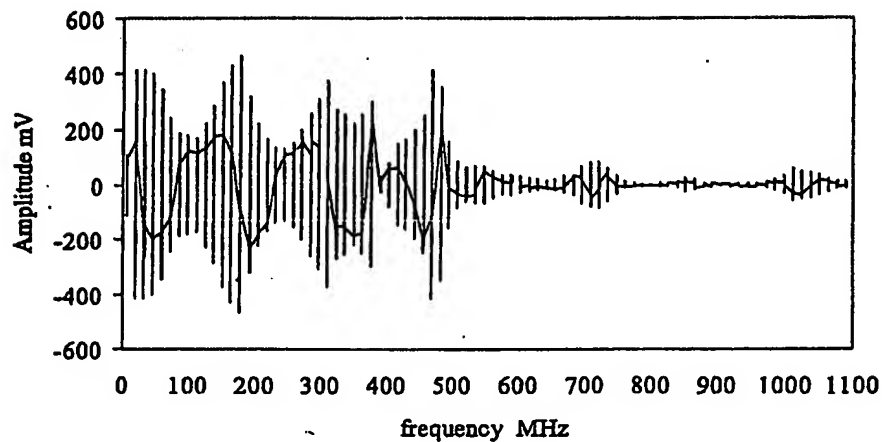
1.09 GHZ



3/4

FIGURE 4

a)



b)

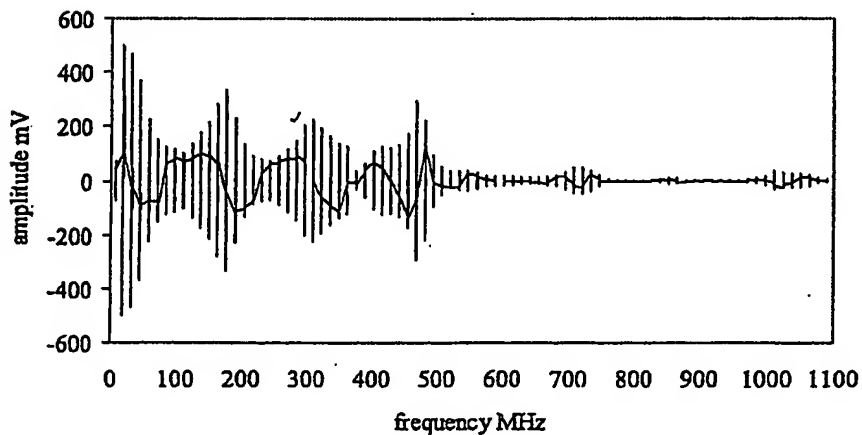


FIGURE 5

